



# Learning Structure of Complex Sensory Inputs with Plasticity in Neural Microcircuits

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## 2 ABSTRACT

3 Synaptic plasticity is explored as a form of unsupervised adaptation in cortical microcircuits to  
4 learn the structure of complex sensory inputs and thereby improve performance of classification  
5 and prediction. The question of whether the structure of specific input patterns is encoded in  
6 the structure of neural networks has been largely neglected. Existing studies that have analyzed  
7 structural adaptation have used simplified, synthetic inputs in contrast to complex and noisy  
8 patterns found in real-world sensory data.

9 In this work, class-specific structural changes are analyzed for three empirically derived models  
10 of plasticity applied to three temporal sensory classification tasks that include complex, real-  
11 world visual and auditory data. Two forms of spike-timing dependent plasticity (STDP) and  
12 the Bienenstock-Cooper-Munro (BCM) plasticity rule are used to adapt the recurrent network  
13 structure before training is performed for pattern recognition tasks.

14 It is shown that plasticity does learn highly input-specific structure in its adaptation. Howe-  
15 ver, it does not improve the performance on sensory pattern recognition tasks due to synaptic  
16 interference between consecutively presented input samples. The changes in synaptic strength  
17 produced by one stimulus are reversed by the presentation of another, thus largely preventing  
18 synaptic changes from being retained in the structure of the network.

19 To solve the problem of interference, we suggest that models of plasticity be extended to restrict  
20 neural activity and synaptic modification to a subset of the neural circuit, which is increasingly  
21 found to be the case in experimental neuroscience.

22 **Keywords:** Synaptic plasticity, spiking neurons, recurrent neural networks, interference, spatiotemporal patterns

## 1 INTRODUCTION

23 Recurrent neural networks consisting of biologically based spiking membrane models have only recently  
24 been applied to real-world learning tasks under a framework called reservoir computing **Buonomano and**  
25 **Maass** (2009); **Maass et al.** (2002). The models of this framework use a recurrently connected set of  
26 neurons driven by an input signal to create a non-linear, high-dimensional temporal transformation of the  
27 input that is used by single layer perceptrons **Rosenblatt** (1958) to produce desired outputs. This restricts  
28 the training algorithms to a linear regression task, while still allowing the potential to work on temporal  
29 data in a non-linear fashion.

30 Given an initially fixed, unchanging connectivity, reservoir computing is based on the principle of ran-  
31 dom projections of the input signal in which the network structure is completely independent of the input

32 patterns. In these models, the only features learned by the trainable parameters of the perceptron readout  
33 are correlations between the randomly projected features and the desired output signal.

34 We believe that learning in neural networks should go farther than supervised training based on error  
35 from the output. All synapses should adapt to be able to encode the structure of the input signal and ideally,  
36 should not rely on the presence of a desired output signal from which to calculate an error with the actual  
37 output. The neural activity generated by the input signal should provide enough information for synapses  
38 to adapt and encode properties of the signal in the network structure. By applying unsupervised adaptation  
39 to the synapses in the form of biologically derived plasticity rules **Bi and Poo** (1998); **Bienenstock et al.**  
40 (1982); **Wittenberg and Wang** (2006) it is hoped to provide the means for the recurrently connected  
41 neurons of the network to learn a structure that generates more effective features than a completely random  
42 projection that is not specific to the input data.

43 In this work we will explore the impact of applying several biologically derived plasticity mechanisms  
44 on three temporal sensory discrimination tasks. Two forms of spike-timing dependent plasticity (STDP)  
45 **Bi and Poo** (1998); **Wittenberg and Wang** (2006) will be tested, along with the Bienenstock-Cooper-  
46 Munro (BCM) rule **Bienenstock et al.** (1982). The sensory tasks will include real-world speech and video  
47 data of human motion. Synaptic plasticity will be applied in an unsupervised pre-training phase, before  
48 the supervised regression of the perceptron readout occurs. We will compare the impact that plasticity has  
49 on the performance in these tasks and also analyze the specific structural adaptation of the weight matri-  
50 ces between each of the classes of input sample in each task. A method will be introduced to evaluate the  
51 extent to which the synaptic changes encode class-specific features in the network structure. Interference  
52 between different samples is a well-established phenomenon in sequentially trained learning models **Fren-**  
53 **nch** (1999); **McCloskey and Cohen** (1989); **Ratcliff** (1990). As this directly concerns neural networks  
54 trained on sensory recognition tasks, a quantification of the interference between the synaptic parameters  
55 will be made for each plasticity model while applied to each task.

56 Existing studies report that adapting neural circuits with plasticity improves their performance on pattern  
57 recognition tasks **Xue et al.** (2013); **Yin et al.** (2012) but there is no analysis of how the adaptation of  
58 synaptic parameters leads to this result. On the other hand, work that does analyze the structural adaptation  
59 of the network does so using synthetic input patterns that are already linearly separable, completely unlike  
60 realistic sensory input **Toutounji and Pipa** (2014). For a review of work applying plasticity models to  
61 improve the function of neural networks, the reader is referred to **Chrol-Cannon and Jin** (2014a).

## 2 RESULTS

### 2.1 DESCRIPTION OF SENSORY INPUTS

62 Complex sensory signals are projected through a common set of nerve fibers to cortical regions that must  
63 learn to distinguish between them based on differences in their spatial-temporal features.

64 Three sensory recognition tasks are selected, among which two of them consist of real audio and video  
65 signals of human speech and motion. For all tasks, the neural network output is trained to respond uniqu-  
66 ely to each of the different types of input sample and therefore be able to perform effective recognition  
67 between them. Also, sample specific synaptic adaptations are analyzed to determine if unique structure is  
68 learned within the network due to synaptic plasticity.

69 The auditory task is to distinguish between nine different speakers based on short utterances of the vowel  
70 /*ae*/. Each of the 640 samples consists of a frequency 'spectrogram' that plots frequency intensity over a  
71 sequence of audio time frames. Figure 1 plots an example sample from each of the nine speakers.

72 The visual task is to distinguish between six types of human behavior; boxing, clapping, waving, wal-  
73 king, running and jogging. The 2391 samples are video sequences of many different subjects performing

74 those six motions. There is a simple pre-processing stage that converts the video data into a sparse repre-  
 75 sentation before being used as input to the neural network. Extracted still frames and processed features  
 76 are plotted in Figure 2 for one subject performing each of the six behaviors.

77 A synthetic data set is generated to model a low spatial dimension but very high frequency temporal  
 78 structure, in contrast to the previous two sensory tasks. Three functions generate time-varying single  
 79 dimensional signals that the network learns to distinguish between. A complete description and method  
 80 for generating the data is described in Jaeger (2007).

81 The auditory and visual tasks are described in Kudo et al. (1999) and Schuld et al. (2004), respectively,  
 82 with data availability also provided.

## 2.2 LEARNING INPUT-SPECIFIC STRUCTURE USING PLASTICITY

83 We wish to test the hypothesis that synaptic plasticity is encoding a distinct structure for input samples of  
 84 different labels. For the speech task, these labels consist of different speakers and for the video recognition  
 85 task the labels consist of different human behaviors.

86 The data sets are divided evenly into two. Each subset is used to train a recurrently connected network  
 87 for 10000 iterations, selecting a sample at random on each iteration. The changes to the weight matrix  
 88 due to plasticity are recorded for each sample presentation. This is then used to create a class-specific  
 89 average weight change for each of the class labels in both of the sample subsets. Finally, we calculate the  
 90 Euclidean distance between each class in one set and each class in the other according to the following  
 91 formula:

$$\text{Dist}(C^X, C^Y) = \sum_{i=1}^N |\Delta W_i(C^X) - \Delta W_i(C^Y)| \quad (1)$$

92 Where  $C$  denote class labels,  $X$  and  $Y$  distinguish the separated sets of samples,  $\Delta W$  is the change in  
 93 weight matrix for a presented sample,  $N$  is the number of synapses, and  $i$  the synapse index.

94 This effectively produces a confusion matrix of similarity in the synaptic weight change for different  
 95 classes of input. Having lower values on the descending diagonal means that there is structural adaptation  
 96 that is specific to the class of that column compared with the similarity between structural adaptations of  
 97 two different classes.

98 Figure 3 shows the 'weight change confusion matrices' described above, for each plasticity model  
 99 applied to all sensory tasks (nine experiments in total). All of the experiments show at least some stronger  
 100 similarity in the descending diagonals and most are stark in this manner. It is certainly a strong enough  
 101 pattern to show that through the many iterations of training, each of the plasticity models have become  
 102 sensitive to the particular structure of the sensory input signals so that each different class of sample will  
 103 give rise to changes in synaptic strength that are distinct from other classes compared with the simila-  
 104 rity to themselves. We re-iterate that the class labels were not used in any way in the plasticity models  
 105 themselves and so the differences in the weight change arise from the input signals alone.

106 There are a few exceptions to the strong diagonal patterns in Figure 3. This means that some classes  
 107 are not effectively distinguished from each other; speakers 8/9 with bi-phasic STDP, behaviors 1/2 with  
 108 BCM, behaviors 1/2/3 and 4/5/6 with tri-phasic STDP. The latter confusion corresponds to the behaviors of  
 109 boxing/clapping/waving and walking/running/jogging. From the similarity of those input features shown  
 110 in the lower panes of Figure 2, it is evident why this confusion might occur.

**Table 1.** Classification Error Rates

	Static	BCM	STDP	TP-STDP
Tri-func	0.153	0.157	0.204	<b>0.138</b>
KTH	<b>0.283</b>	0.3	0.333	0.383
Vowels	0.089	<b>0.086</b>	0.092	<b>0.086</b>

**Table 2.** Synaptic Interference

	BCM	STDP	TP-STDP
Tri-func	0.82	<b>0.8</b>	0.88
KTH	<b>0.92</b>	0.93	0.96
Vowels	0.96	<b>0.58</b>	0.9

## 2.3 CLASSIFICATION PERFORMANCE WITH PLASTICITY

111 Perhaps the ultimate goal of neural network methods when applied to sensory tasks is the ability to accu-  
 112 rately distinguish different types of input sample by their patterns. We compare the error rates achieved  
 113 by our neural network on the three sensory tasks, with and without the different forms of plasticity used in  
 114 this work. Table 1 lists the error rates achieved for each of the learning tasks with the different plasticity  
 115 rules active in a pre-training phase in addition to a static network with fixed internal synapses.

116 From the error rates in Table 1 it is evident that pre-training the network with synaptic plasticity can  
 117 make insignificant improvements in lowering the error rate. However, the results here indicate that it can  
 118 have a greater negative impact than a positive one. In the KTH human behavior data set, all three plasticity  
 119 models increase the error rate by between 1.7% and 10%. Conversely, the best improvement was found  
 120 on the tri-function signal recognition task with tri-phasic STDP at only 1.5%.

121 It is clear from the network output that pre-training with synaptic plasticity is not a suitable method  
 122 for this class of model, This does not contradict the result that plastic synapses are learning useful, input-  
 123 specific structure. However, it does suggest that the structure being learned is not effectively utilized in the  
 124 generation of a network output. We next investigate interference between synaptic changes to determine  
 125 if the structural learning is retained in the network or if interference is a barrier for effective application  
 126 of synaptic plasticity.

## 2.4 SYNAPTIC INTERFERENCE

127 When a model adapts incrementally to sequentially presented input, existing patterns that have been  
 128 learned by the model parameters are prone to be overwritten by learning new patterns. This is known  
 129 as interference. The work that has studied this effect **French** (1999); **McCloskey and Cohen** (1989);  
 130 **Ratcliff** (1990), test the ability to recognize previously presented input after the model has been trained  
 131 on new ones in order to estimate how much learning has been undone. When new training leaves the  
 132 model unable to recognize old patterns, it is said there has been catastrophic interference and forgetting.

133 We introduce a method of measuring interference directly in synaptic parameters instead of the model  
 134 output. Our measure is described in detail in the Methods section.  $I^{total}$  directly quantifies all synaptic  
 135 changes that are overwritten.

136 The interference for each of our experiments is listed in Table 2. In all but one of the experiments  
137 the interference level is between 82% and 96%. Most of the learned structure for each class of input is  
138 forgotten as consecutive samples overwrite each other's previous changes. Bi-phasic STDP applied to  
139 speaker recognition has the lowest level of interference at 58%.

140 To further explore interference and visualize the impact of plasticity, synaptic changes will be analyzed  
141 directly. Figure 4 is an illustrative example for the speaker recognition task with BCM plasticity (similar  
142 figures for the other experiments are given in S1–S8). It shows the adaptation of the synaptic weight  
143 matrix produced by each speaker in the voice recognition task. This is plotted against the activity level for  
144 each neuron,  $\mathbf{S}$ , and the readout weights,  $\mathbf{R}$ , that are trained to generate an output that is sensitive to that  
145 given speaker. Each of these sub plots is the average response taken over all sample presentations from  
146 that speaker. This makes a whole chain of effect visible: from the synaptic change of an internal network  
147 connection, to the average neuron state for a given speaker, to the selective weights of the readout for that  
148 speaker. For all to be working well in a cohesive system, we expect that a positive weight change should  
149 correspond with a neuron activation unique to the class which would in turn improve the recognition  
150 ability of the readout to identify that class.

151 The sections of the class weight matrix highlighted in green in Figure 4, highlight an example where  
152 synaptic interference is occurring between different types of pattern. Directly opposing features in the  
153 weight matrix adaptations show the samples negating each other's changes. However, the same features  
154 are also most distinctively class specific.

155 Any synapse can only change in two directions: positively or negatively, which means that a single  
156 synapse can only adapt to distinguish between two mutually exclusive kinds of input pattern. If  $n$  synapses  
157 are considered in combination, then the number of input patterns that can be discriminated becomes  
158  $2^n$  in ideal theoretical conditions. Figure 4 illustrates this principle in practice with regards to the nine  
159 speaker recognition tasks. The adapted synapses labeled (a) can clearly distinguish speaker  $\{\#1\}$  from  
160 speakers  $\{\#2, \#3\}$  but cannot distinguish  $\{\#2\}$  from  $\{\#3\}$ . Similarly, the adapted synapses labeled  
161 (b) can distinguish speakers  $\{\#1, \#6, \#8\}$  from speakers  $\{\#3, \#4, \#9\}$  but cannot distinguish speakers  
162 within either of those sets. However, if the synapses (a), (b), (c) and (d) are considered in combination,  
163 then all speakers can be distinguished by synaptic plasticity changes alone.

164 Figure 4 also shows the weight changes are not correlated with the neural activity or readout weights.  
165 For plasticity to improve the accuracy of sensory discrimination, it would be expected that synapses would  
166 strengthen for class specific neural activity and weaken for common neural activity. This is not the case  
167 in our results.

### 3 DISCUSSION

#### 3.1 UNSUPERVISED PLASTICITY LEARNS LABEL SPECIFIC STRUCTURE

168 Both STDP and BCM models adapt the synapses of a network in distinctive patterns according to which  
169 type of sample is being presented to the network. We can conclude that presenting a training signal  
170 with the sample label is not required for plasticity to learn specific information for complex sensory  
171 inputs from different sources. This result holds for the speech, visual and benchmark pattern recognition  
172 tasks. To achieve this feat, we hypothesize that plasticity drives the synaptic parameters to a structure that  
173 represents an average between all input samples. Once converged, any further input stimulus will drive  
174 the synaptic parameters in a unique direction away from this average structure. On balance, scrambled  
175 presentation of random inputs keeps the network in this sensitive state.

### 3.2 UNIFORMLY APPLIED PLASTICITY LEADS TO SYNAPTIC INTERFERENCE

176 We show synaptic plasticity spends most of its action counter-acting previous changes and overwriting  
177 learned patterns. The same patterns of synaptic adaptation that distinctly characterizes each class of input  
178 are the same ones that reverse adaptations made by other inputs.

179 Plasticity is applied uniformly to all synapses. All neurons in a recurrent network produce activity when  
180 given input stimulus. Combined, these factors mean that any input sample will cause the same synapses  
181 to change. This leads to synaptic competition, interference and ultimately, forgetting.

### 3.3 LOCALITY OF PLASTICITY REQUIRED TO OVERCOME INTERFERENCE

182 To overcome the problem of interference, the mechanisms of plasticity need to be restricted to adapt only  
183 a subset of the synapses for any given input stimulus. There is much existing research that supports this  
184 conclusion and a number of possible mechanisms that can restrict the locality of plasticity.

185 It has been shown *in vivo* (using fMRI and neurological experiment) that synaptic plasticity learns  
186 highly specific adaptations early in the visual perceptual pathway **Karni and Sagi** (1991); **Schwartz**  
187 **et al.** (2002). Simulated models of sensory systems have demonstrated that sparsity of activity is essential  
188 for sensitivity to input-specific features **Barranca et al.** (2014); **Finelli et al.** (2008). In fact, in a single-  
189 layer, non-recurrent structure, STDP is shown to promote sparsity in a model olfactory system **Finelli**  
190 **et al.** (2008). Conversely, in recurrent networks, STDP alone is unable to learn input specific structure  
191 because it 'over-associates' **Bourjaily and Miller** (2011). Strengthened inhibition was used to overcome  
192 this problem and combined with reinforcement learning to produce selectivity in the output **Bourjaily and**  
193 **Miller** (2011). By promoting sparsity, the lack of activity in most of the network will prevent activity-  
194 dependent models of plasticity in adapting those connections.

195 Reward modulated plasticity has also been widely explored in simulated **Darshan et al.** (2014); **Gavor-**  
196 **nik et al.** (2009) and biological experiment **Lepousez et al.** (2014); **Li et al.** (2013). Input-specific  
197 synaptic changes are shown to be strongest in the presence of a reward signal **Gavornik et al.** (2009);  
198 **Lepousez et al.** (2014). Lasting memories (synaptic changes not subject to interference), are also seen  
199 to rely on a process of re-consolidation consisting of fear conditioning **Li et al.** (2013). A reinforcement  
200 signal based on either reward or fear conditioning can be effectively used to restrict synaptic changes in a  
201 task dependent context such as sensory pattern recognition.

202 Another way to restrict synaptic changes in a task dependent way is to rely on a back-propagated error  
203 signal that has well established use in artificial neural networks. This might be achieved in a biologically  
204 plausible way through axonal propagation **Kempton et al.** (2001) or top-down cortical projections sending  
205 signals backwards through the sensory pathways **Schfer et al.** (2007). Top-down neural function in general  
206 is thought to be essential in determining structure in neural networks **Sharpee** (2014), providing a context  
207 for any adaptations.

208 Neural cascades **Polat and Sagi** (1994) and synchronicity **Hoppensteadt** (1989) have also been  
209 suggested as factors that enable input-specific plasticity.

### 3.4 LEARNING INPUT STRUCTURE DOES NOT NECESSARILY IMPROVE PERFORMANCE

210 Structural adaptation with plasticity in the pre-training phase, while specific, may not be utilized by the  
211 output produced by the network readout. This could be due to the following reasons. Firstly, there is a  
212 disparity in the neural code. The output from a recurrent spiking network model is currently decoded as a  
213 rate code. In contrast, synaptic plasticity updates structure in a way that depends on the precise temporal  
214 activity of neural spikes. Secondly, information content is reduced. While creating associations between  
215 co-activating neurons, Hebbian forms of plasticity may also increase correlations and reduce information  
216 and separation. These can determine the computational capacity of a recurrent network model **Chrol-**  
217 **Cannon and Jin** (2014b). Both discrepancies could be barriers for the effective application of plasticity

218 to improve pattern recognition. Therefore new frameworks of neural processing should be based directly  
 219 on the adapting synapses. This will lead to functional models of neural computing that are not merely  
 220 improved by synaptic plasticity, but that rely on it as an integral element.

## 4 MATERIAL & METHODS

### 4.1 NEURAL MICROCIRCUIT

221 The neural network model used in this work is illustrated in Figure 5. Recurrently connected neurons,  
 222 indicated by  $L$  are stimulated by the inputs directly as injected current,  $I$ , that perturbs the membrane  
 223 potential modeled with a simple model **Izhikevich** (2003). This method for modeling the spiking activity  
 224 of a neuron is shown to reproduce most naturally occurring patterns of activity **Izhikevich** (2004). The  
 225 real-valued inputs are normalized between 0 and 1, which are multiplied by a scaling factor of 20 before  
 226 being injected as current into  $L$ . Input connections number  $0.2 \cdot \text{network size}$ , projected randomly to the  
 227 network nodes. The network activity dynamics are then simulated for  $30ms$ . Then, the resulting spike  
 228 trains produced by each of the neurons is passed through a low-pass filter,  $f$ , to produce a real valued  
 229 vector used to train a linear readout with the iterative, stochastic gradient descent method.

230 For our experiments the network consists of 35–135 spiking neurons with the ratio of excitatory to  
 231 inhibitory as 4:1. Neurons are connected with static synapses i.e. the delta impulse (step) function. Con-  
 232 nectivity is formed by having  $N^2 \cdot C$  synapses that each have source and target neurons drawn according to  
 233 uniform random distribution, where  $N$  is the number of neurons and  $C$  is the probability of a connection  
 234 between any two neurons. Weights are drawn from two Gaussian distributions;  $\mathcal{N}(6, 0.5)$  for excitatory  
 235 and  $\mathcal{N}(-5, 0.5)$  for inhibitory. When plasticity adapts the reservoir weights,  $w_{max}$  is clamped at 10 and  
 236  $w_{min}$  at  $-10$ . All parameters for excitatory and inhibitory neuron membranes are taken from **Izhikevich**  
 237 (2003). The equations for the membrane model are as follows:

$$v' = 0.04v^2 + 5v + 140 - u + I \quad (2)$$

$$u' = a(bv - u) \quad (3)$$

238 With the spike firing condition:

$$\text{if } v > 30mV \quad \text{then} \quad \begin{cases} v \leftarrow c \\ u \leftarrow u + d \end{cases} \quad (4)$$

239 To generate a real-valued output from the discrete spiking activity, the spike train from each neuron is  
 240 low-pass filtered according to Equation 5. The vector of values produced is then weighted with the readout  
 241 weight matrix and summed to produce a single output value, shown in Equation 6.

$$x_i = f(S(t)) = \sum_{t=1}^T \exp\left(\frac{-t}{\tau}\right) \cdot w_{max} \quad (5)$$

$$y = \sum_{i=1}^n x_i \cdot w_i \quad (6)$$

242 The state vector for a neuron is denoted by  $x_i$ , the filter function is  $f()$  and the spike train is  $S(t)$ . The  
 243 maximum number of time-steps in  $S(t)$  is  $T$ , in this case 50. The decay constant  $\tau$  is 6.

244 This output weights are updated according to the iterative, stochastic gradient descent method: Least  
245 Mean Squares, given in Equation 7.

$$w_i \longleftarrow w_i + \mu(d - y)x_i. \quad (7)$$

246 Here,  $d$  is the desired output,  $y$  is the actual output,  $x_i$  is the input taken from a neuron's filtered state,  
247 and  $\mu$  is a small learning rate. The weight from  $x_i$  to the output is  $w_i$ .

## 4.2 SYNAPTIC PLASTICITY MODELS

248 Three synaptic plasticity mechanisms are employed in this study, each of them based on the Hebbian  
249 postulate **Hebb** (1949) of “neurons that fire together, wire together”. Each mechanism is outlined as  
250 follows:

251 **BCM Plasticity:** The BCM rule **Bienenstock et al.** (1982) is a rate based Hebbian rule that also regula-  
252 tes the post-neuron firing rate to a desired level. It works on a temporal average of pre- and post-synaptic  
253 activity. The BCM rule is given in Equation 8. The regulating parameter is the dynamic threshold  $\Theta_M$ ,  
254 which changes based on the post-synaptic activity  $y$  and the desired level  $y_0$  in the following relationship:  
255  $E[y/y_0]$ , where  $E[\cdot]$  denotes a temporal average. There is also a decay parameter  $\epsilon w_i$  for additional sta-  
256 bility, that slowly reduces connection strength and so provides a mechanism for uniform weight decay,  
257 irrespective of the level of activity or correlation. A plot of the BCM weight change is presented in Figure  
258 S9 in Supporting Information.

$$\frac{dw_i}{dt} = y(y - \theta_M)x_i - \epsilon w_i \quad (8)$$

259 **Bi-phasic STDP:** The STDP rule depends on the temporal correlation between pre- and post-synaptic  
260 spikes. The synaptic weight change is computed based on the delay between the firing times of the pre-  
261 and post- neuron. This is described in a fixed 'learning window' in which the y-axis is the level of weight  
262 change and the x-axis is the time delay between a pre- and post-synaptic spike occurrence. The bi-phasic  
263 STDP rule consists of two decaying exponential curves **Song et al.** (2000), a positive one to potentiate in-  
264 order spikes, and a negative one to depress out-of-order spikes. This rule was derived from experimental  
265 work carried out on populations of neurons *in vitro* **Markram et al.** (1997)**Bi and Poo** (1998). Bi-phasic  
266 STDP is given in Equation 9.

$$\Delta w(t) = \begin{cases} A_+ \cdot \exp\left(\frac{-\Delta t}{\tau_+}\right) & \text{if } t > 0 \\ A_- \cdot \exp\left(\frac{\Delta t}{\tau_-}\right) & \text{if } t \leq 0 \end{cases} \quad (9)$$

267 **Tri-phasic STDP:** A tri-phasic STDP learning window consists of a narrow potentiating region for  
268 closely correlated activity but depressing regions on either side: for recently uncorrelated activity, and  
269 for correlated but late activity. This learning window has been observed *in vitro*, most notably in the  
270 hippocampi, between areas CA3 and CA1 **Wittenberg and Wang** (2006). The tri-phasic STDP is given  
271 in Equation 10.

$$\Delta w(t) = A_+ \cdot \exp\left(\frac{-(x - 20)^2}{200}\right) - A_- \cdot \exp\left(\frac{-(x - 20)^2}{2000}\right) \quad (10)$$

272 Both STDP learning windows are plotted in Figure S10 in Supporting Information.

## 4.3 SYNAPTIC INTERFERENCE MEASURE

273 We wish to quantify interference directly between synaptic changes of plasticity. Our formulation of  
274 synaptic interference is based on the synaptic changes from sequentially presented samples. Changes for

275 a given type of sample are called  $\Delta W_t$  and changes for all others are  $\Delta W_o$ . Interference must be calculated  
 276 individually for each type of sample,  $I_t^{class}$ , and averaged together to get the overall interference,  $I^{total}$ .  
 277 The equations are as follows:

$$I_t^{class} = \sum_{i=1}^N \frac{1}{N} [\Delta W_{ti} \cdot \Delta W_{oi} < 0][|\Delta W_{ti}| < |\Delta W_{oi}| \cdot C] \quad (11)$$

$$I^{total} = \sum_{t=1}^C \frac{I_t^{class}}{C} \quad (12)$$

278 Where  $I$  is interference,  $N$  is the number of synapses,  $C$  is the number of competing sample types and  
 279  $\Delta W$  is a vector of synaptic changes. Subscript  $i$  denotes the parameter index, subscript  $t$  denotes samples  
 280 of a given type and subscript  $o$  denotes samples of all other types.

#### 4.4 SYNTHETIC SIGNAL DATA

281 A synthetic benchmark task is taken from a study performed with Echo State Networks **Jaeger** (2007), a  
 282 similar type of network model to the one we employ, but using artificial neurons instead. The task is to  
 283 predict which of three signal generating functions is currently active in producing a time-varying input  
 284 signal. To generate a sample of the signal at a given time step, one of the three following function types  
 285 is used; 1) A sine function of a randomly selected period, 2) A chaotic iterated tent map, 3) A randomly  
 286 chosen constant. The generator is given some low probability, 0.05, of switching to another function at  
 287 each time-step. The full method of generating the data is described in **Jaeger** (2007).

#### 4.5 SPEAKER RECOGNITION DATA

288 A speaker recognition task is a classification problem dealing with mapping time-series audio input data  
 289 to target speaker labels. We use a data set taken from **Kudo et al.** (1999) which consists of utterances of  
 290 9 male Japanese speakers pronouncing the vowel /ae/. The task is to correctly discriminate each speaker  
 291 based on the speech samples. Each sample is comprised of a sequence of 12 feature audio frames. The  
 292 features of each frame are the LPC cepstrum coefficients. The sample sequence ranges between 7-29  
 293 frames. The dataset is divided into training and testing sets of 270 and 370 samples each, respectively.  
 294 Note that unlike the benchmark data used in this report, the samples are not in a consecutive time-series,  
 295 yet each sample consists of a time-series sequence of audio frames.

#### 4.6 PRE-PROCESSING OF THE HUMAN MOTION DATA

296 A visual task is selected to test high dimensional spatial-temporal input data. The KTH data set **Schuldt**  
 297 **et al.** (2004) consists of 2391 video files of people performing one of six actions; boxing, clapping,  
 298 waving, walking and jogging. There are 25 different subjects and the samples cover a range of conditi-  
 299 ons that are described in more detail in **Schuldt et al.** (2004). Each video sample is taken at 25 frames  
 300 per second and down sampled to a resolution of 160x120 pixels. We process the raw video sequences  
 301 according to a formula shown in the following equations:

$$M(t) = \|\Delta(I_1, I_2), \dots, \Delta(I_{N-1}, I_N)\| \quad (13)$$

$$M(t, i) = \begin{cases} 1 & \text{if } M(t, i) \geq 0.2 \cdot \max(M(\cdot)) \\ 0 & \text{else} \end{cases} \quad (14)$$

302 The final input matrix  $M$  is indexed by time-frames,  $t$  and spatial samples  $i$ . Column vectors  $I_n$  are  
 303 individual frames, re-shaped into one dimension. Each sample contains up to a total of  $N$  frames. In plain  
 304 language, this process essentially further down samples by a factor of 0.2 and calculates the difference  
 305 between pixels in consecutive frames, which are then used as the new input features. Each frame is then  
 306 re-shaped into a single dimensional column vector then appended together to form an input matrix in  
 307 which each column is used as the neural network input at consecutive time steps. Figure 2 shows frames  
 308 extracted from an example of each type on motion along with the corresponding processed features.

## DISCLOSURE/CONFLICT-OF-INTEREST STATEMENT

309 The authors declare that the research was conducted in the absence of any commercial or financial  
 310 relationships that could be construed as a potential conflict of interest.

## AUTHOR CONTRIBUTIONS

311 Conception and design of the work was by YJ and JCC. Experiments were performed by JCC. Analysis  
 312 and interpretation were undertaken by JCC and YJ. Manuscript was written by JCC and revised by YJ.

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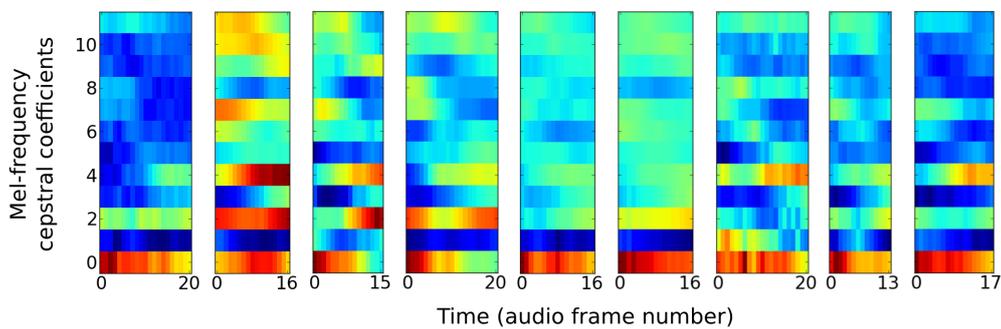
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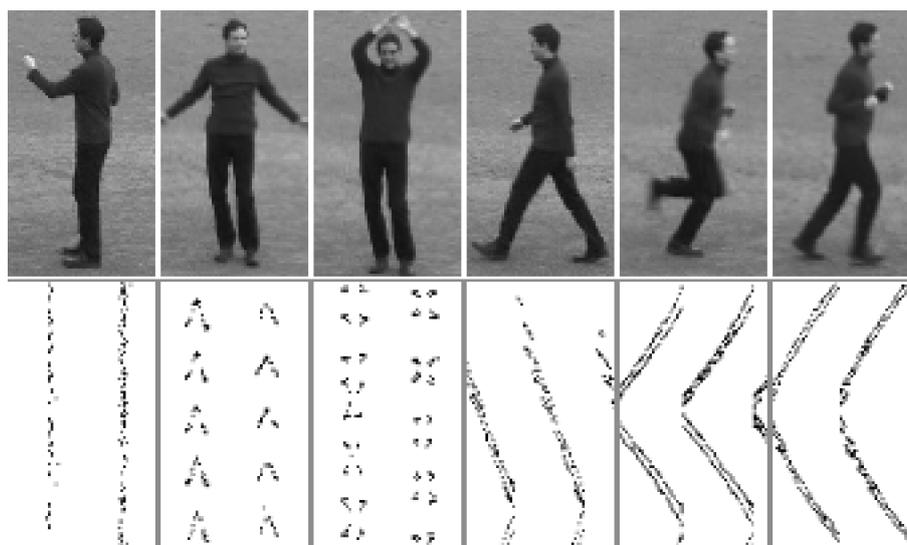
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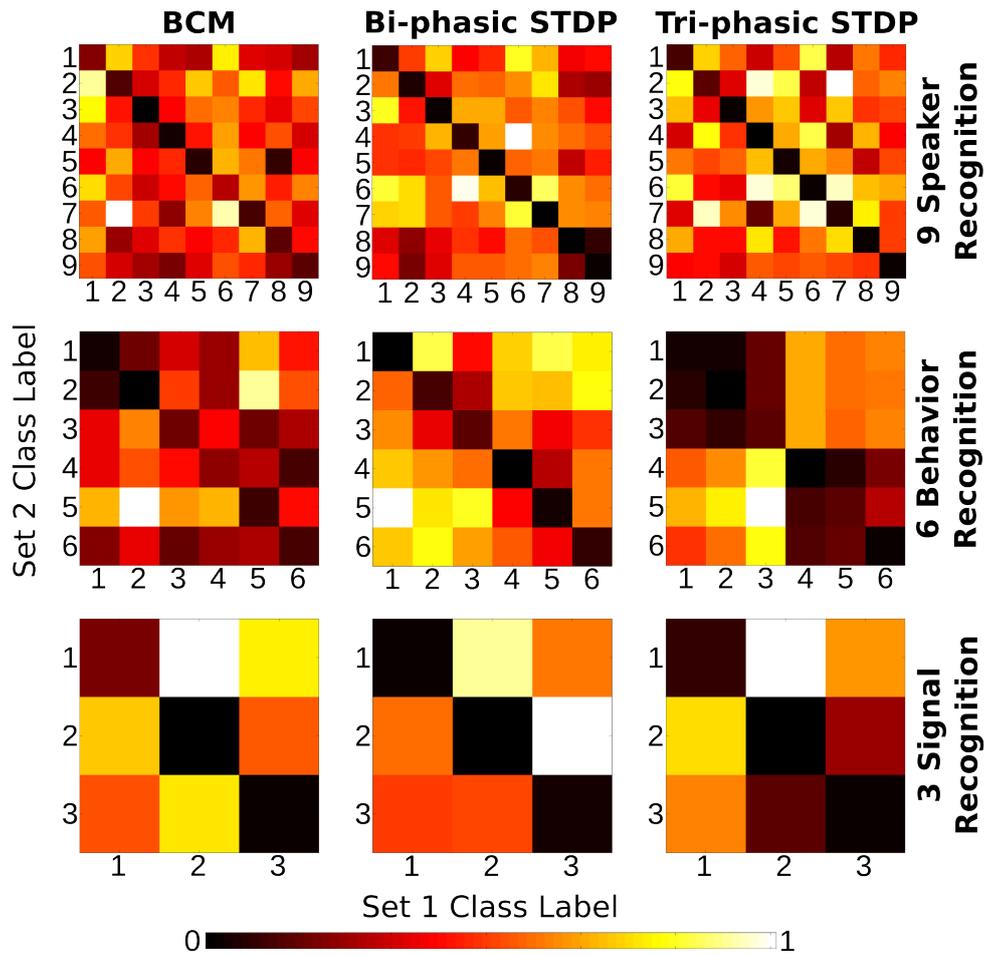
## FIGURES



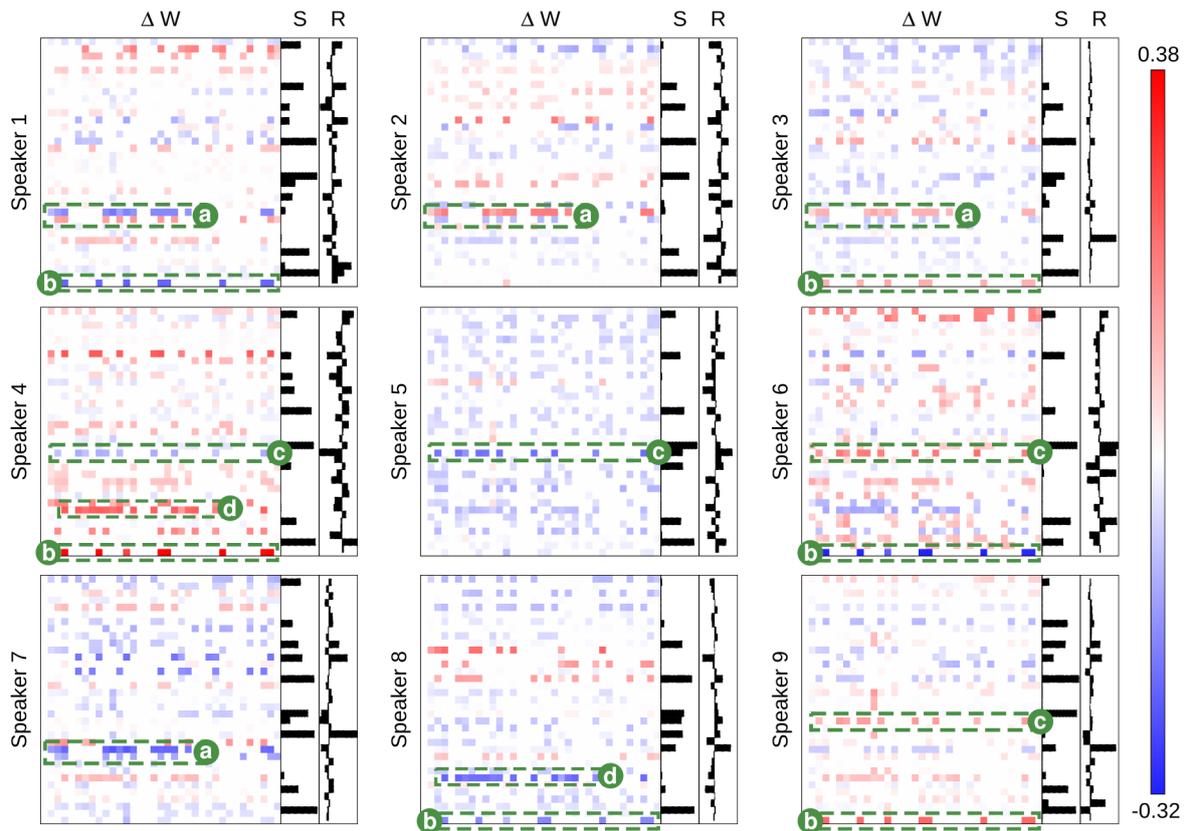
**Figure 1.** Vowel samples from the nine speakers in the speaker recognition task. The audio signals in the data set are pre-processed into 12 Mel-frequency cepstrum coefficients (MFCC) features. Samples from each speaker have variable time duration in the number of audio frames they consist of.



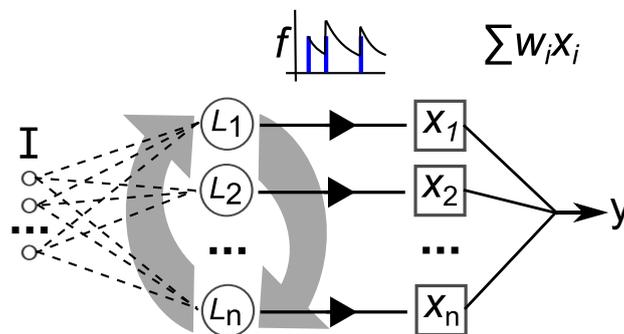
**Figure 2.** Human motion samples for the six types of behavior in the KTH visual discrimination task. This illustration consists of different behaviors from a single person, while the whole data set contains 25 persons. **Top row:** Still frames from example video samples; boxing, clapping, waving, walking, running and jogging. **Bottom row:** Features extracted corresponding to the samples above. Features are the raw time-series activity used as input to the neural network.



**Figure 3.** Class correlation of structural synaptic adaptation. Heat map plots indicate the structure learned on each class for the three tasks under each of the plasticity rules. Essentially, it is a confusion matrix of the geometric distance between the weight matrix adaptation of each class of sample. The training data for each task is divided into two sets. Class-average adaptation is found for each set. There is then a distance calculated between each class of the two sets. Lower values on the descending diagonal indicate higher correlation within a class adaptation and therefore strong class-specific structure learned.



**Figure 4.** The class-specific synaptic adaptation for the 9 class speaker recognition task under BCM plasticity. The main heat maps in each subplot show the adaptation of the weight matrix (synapses) after the presentation of voice input data from each speaker. Blue values show a reduction in synaptic strength and red values show an increase. The bar-chart, **S**, shows the average neuron activation for each class. The bar-chart, **R**, shows the learned readout weights. Labeled synapses **a, b, c, d** indicate key structural changes that are selective between different speakers. Each label alone can distinguish between two sets of speaker. Taken all together, the labeled synapses adapt specifically to each speaker in a unique pattern, learning a distinct network structure for each one.



**Figure 5.** Depiction of the elements of our recurrent network model. **I** is a multi-dimensional input signal, **L** nodes constitute the recurrent network, the **x** vector is the neural activation state, **f** is the filtering of the spike trains and **y** is the output after weight and sum.